



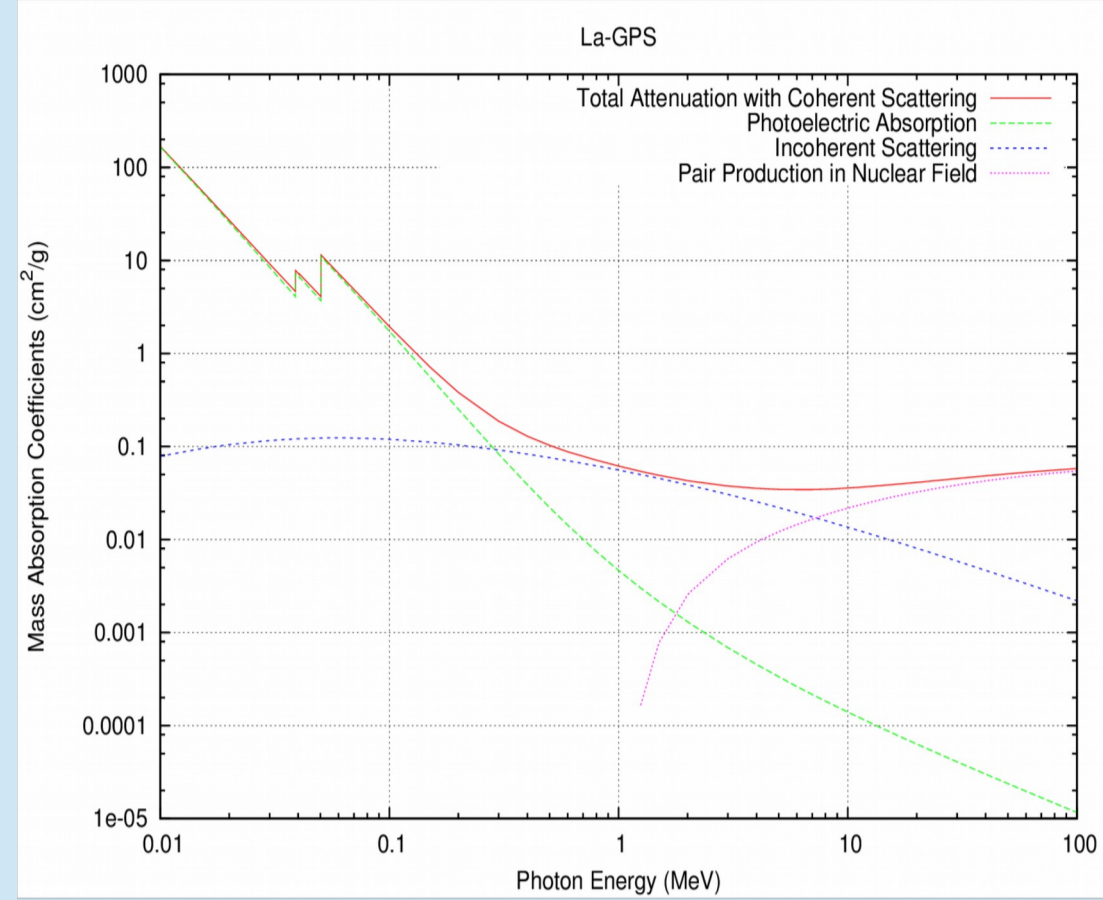
Evaluation of Position Resolution for a Prototype Whole-Body PET Detector Based on Suppressing Backgrounds by Compton Scattering

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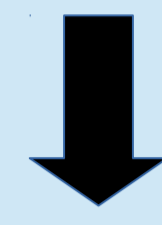
Abstract — The detector with high-growth-rate (HGR) La-GPS and wave-length sifting fiber (WLSF) has sufficient ability for PET in spite of its lower cost. Energy resolution is 31.4%, and position resolution is 1.04 mm. In simulation, our system with parameters from experiment can identify 3 mm cancer.

Introduction



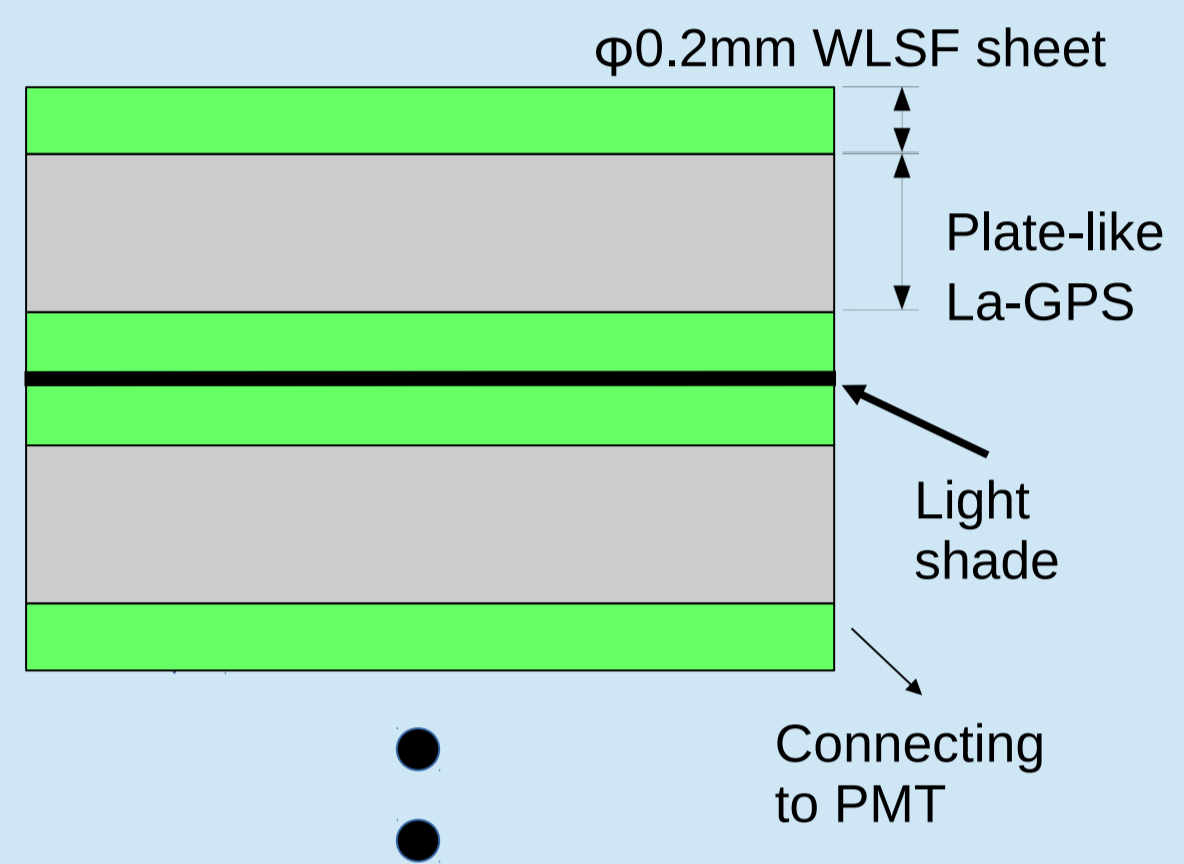
Photon cross section in scintillator [1]

- In scintillator, Compton scattering occur 4 times as much as photoelectric absorption with 0.511 MeV gamma-ray [1]
- Compton scattering makes PET's images unclear.

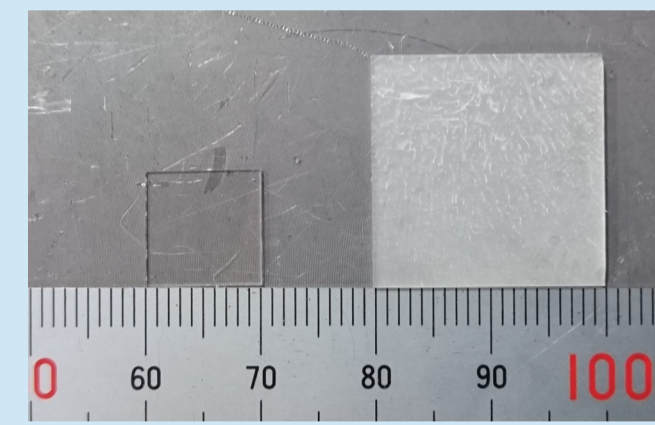


Identifying scattering events is important for PET.

Our detector



Layers of Plate-like HGR La-GPS and WLSF
•HGR La-GPS
Lower cost (about one-fifth the cost of normal crystals)

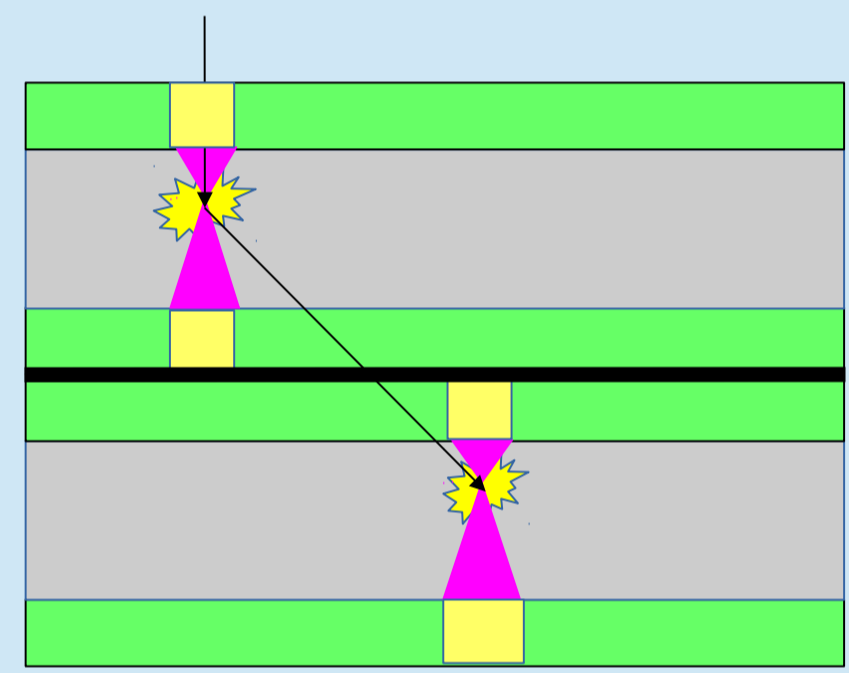


Left : Normal-crystal (1 cm × 1 cm)
Right : HGR crystal (2 cm × 2 cm)

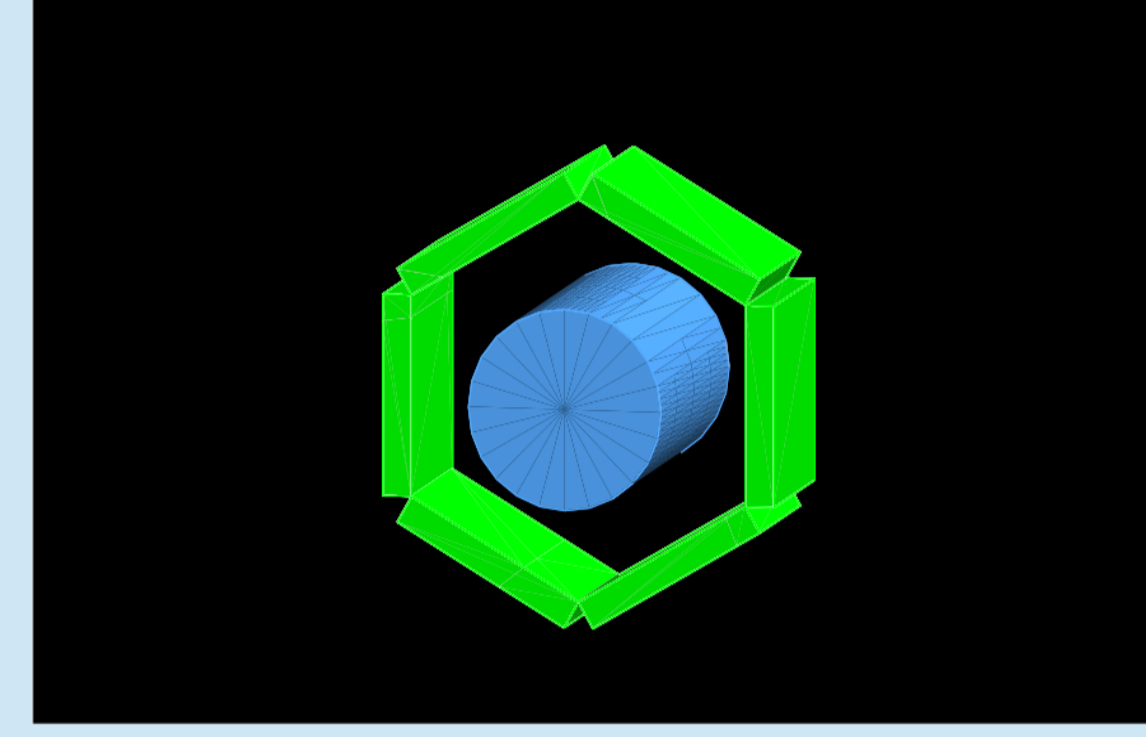
- Layers
Measuring Z-component and identifying scattering event
- WLSF
Measuring X- (top surface) , Y- (bottom surface) component and energy deposit

Identifying and analysis method

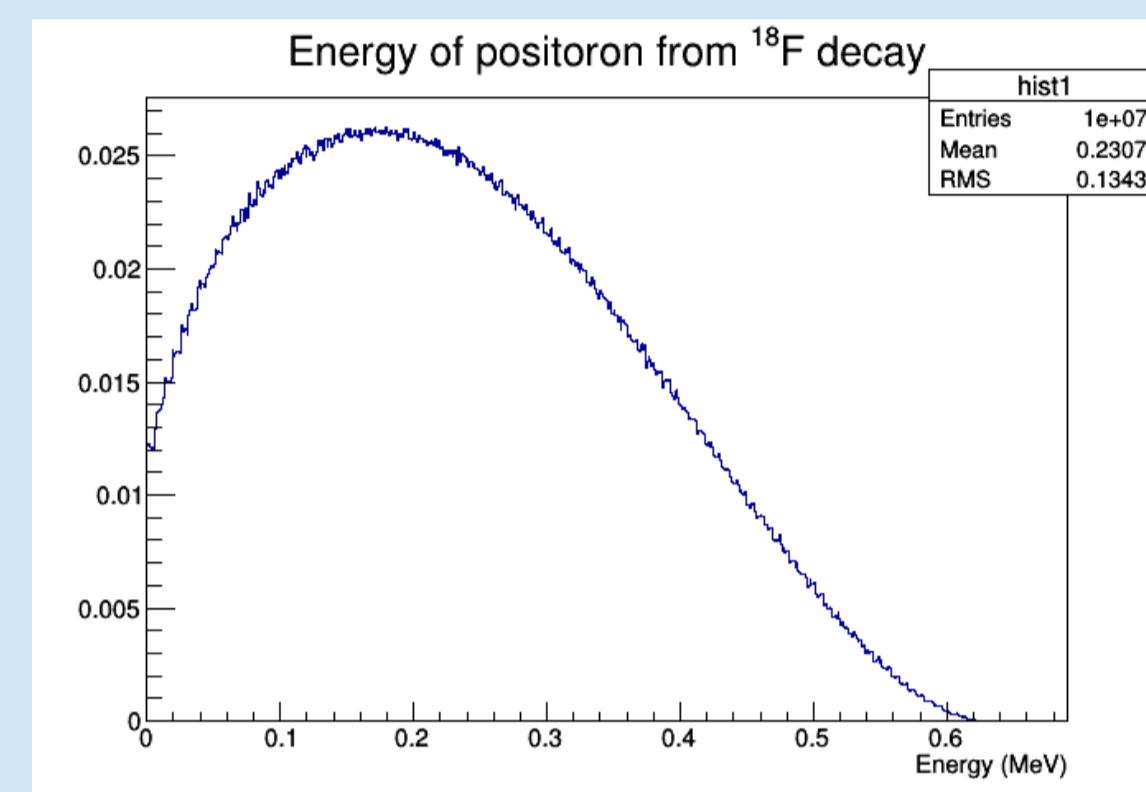
- Signals from plural layers
- Considering as a scattering event
- Regarding the nearest point to the body as the first emission point



Simulation (GEANT4)



Parameter	Quantity
Radioactivity concentration (normal tissue)	2 Mbq/kg
Radioactivity concentration (cancer)	10 Mbq/kg
Width resolution	1 mm
Depth resolution	1 mm
Energy resolution	31.4% (FWHM)
Time resolution	no error



Setting

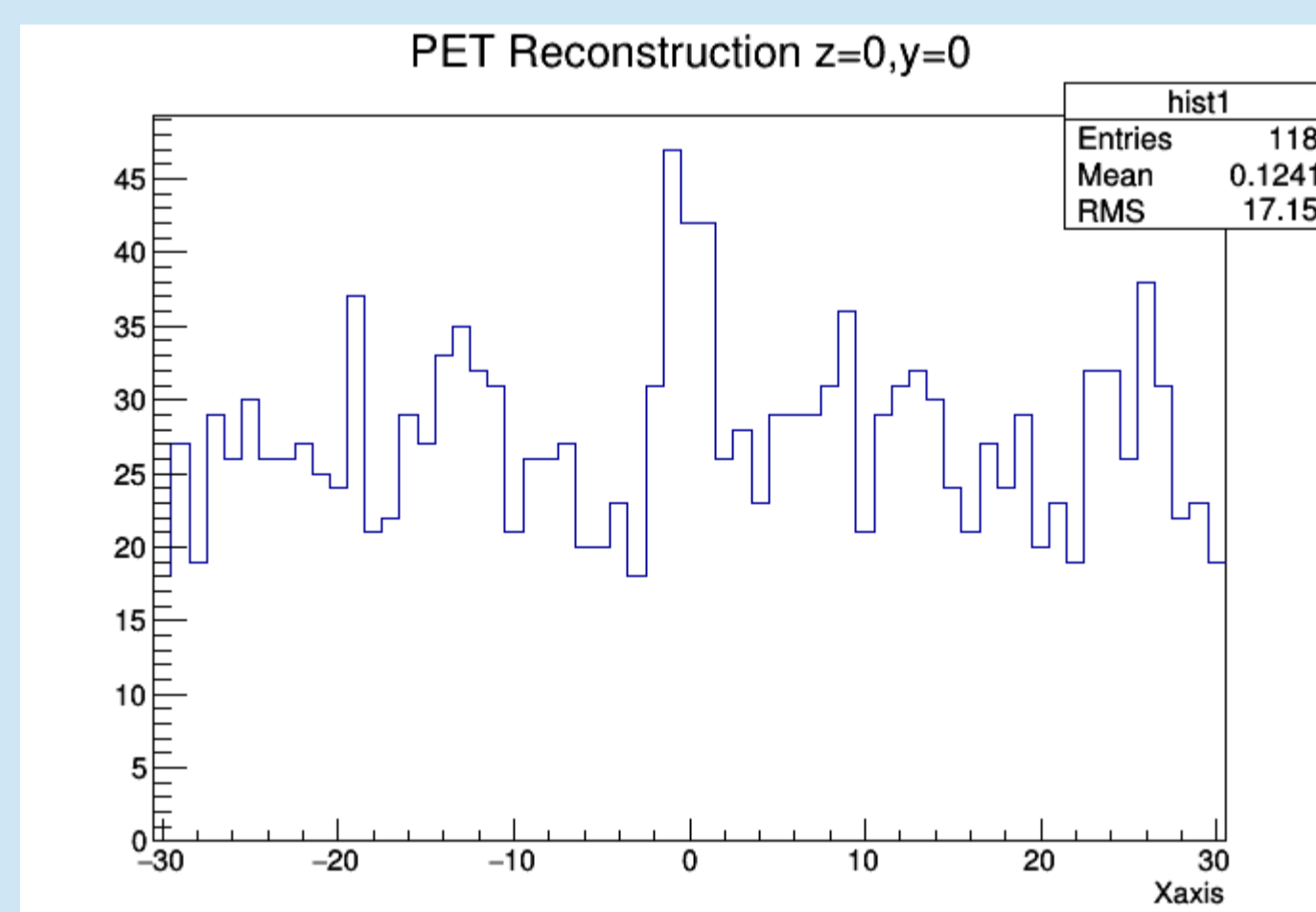
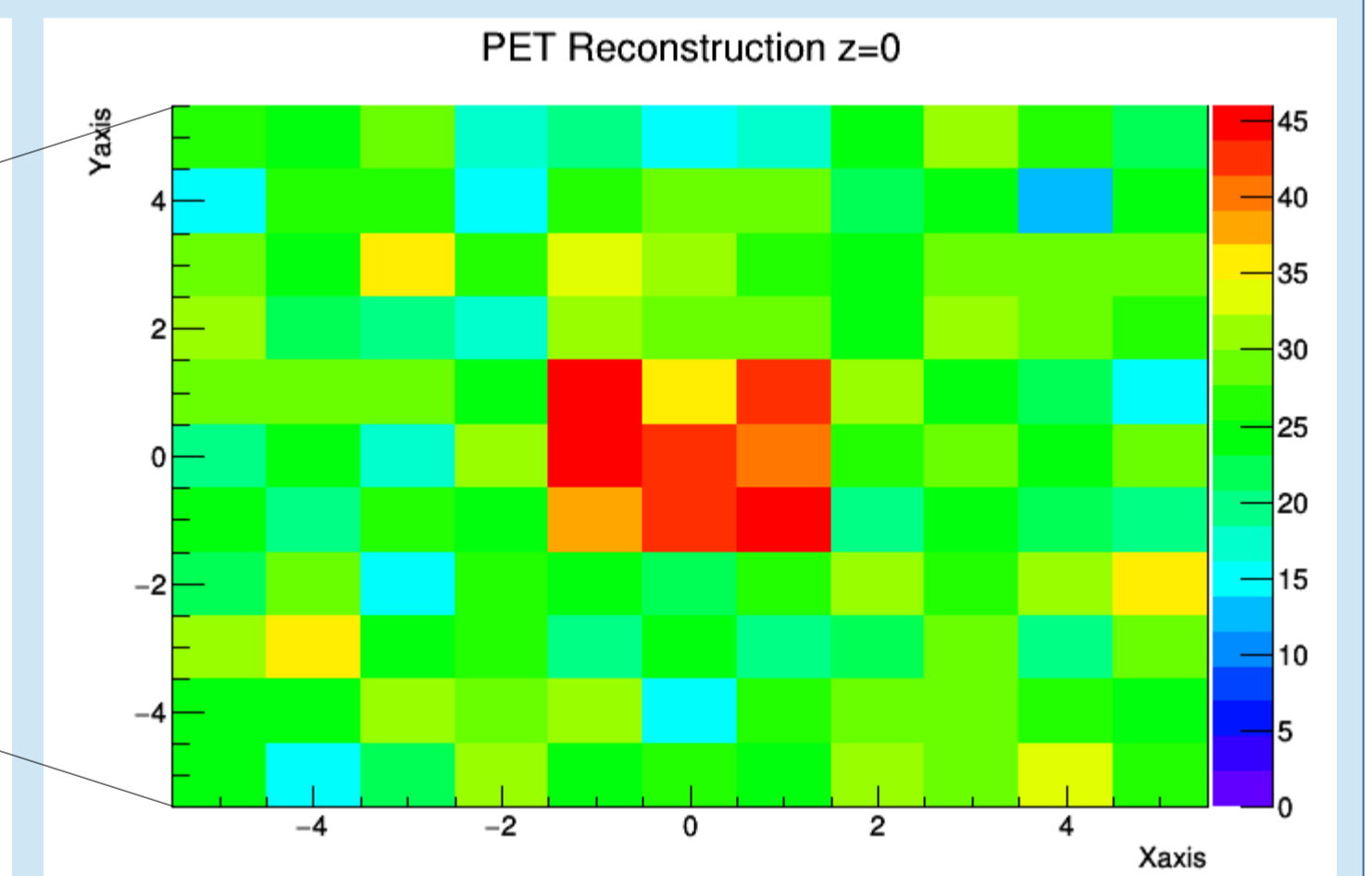
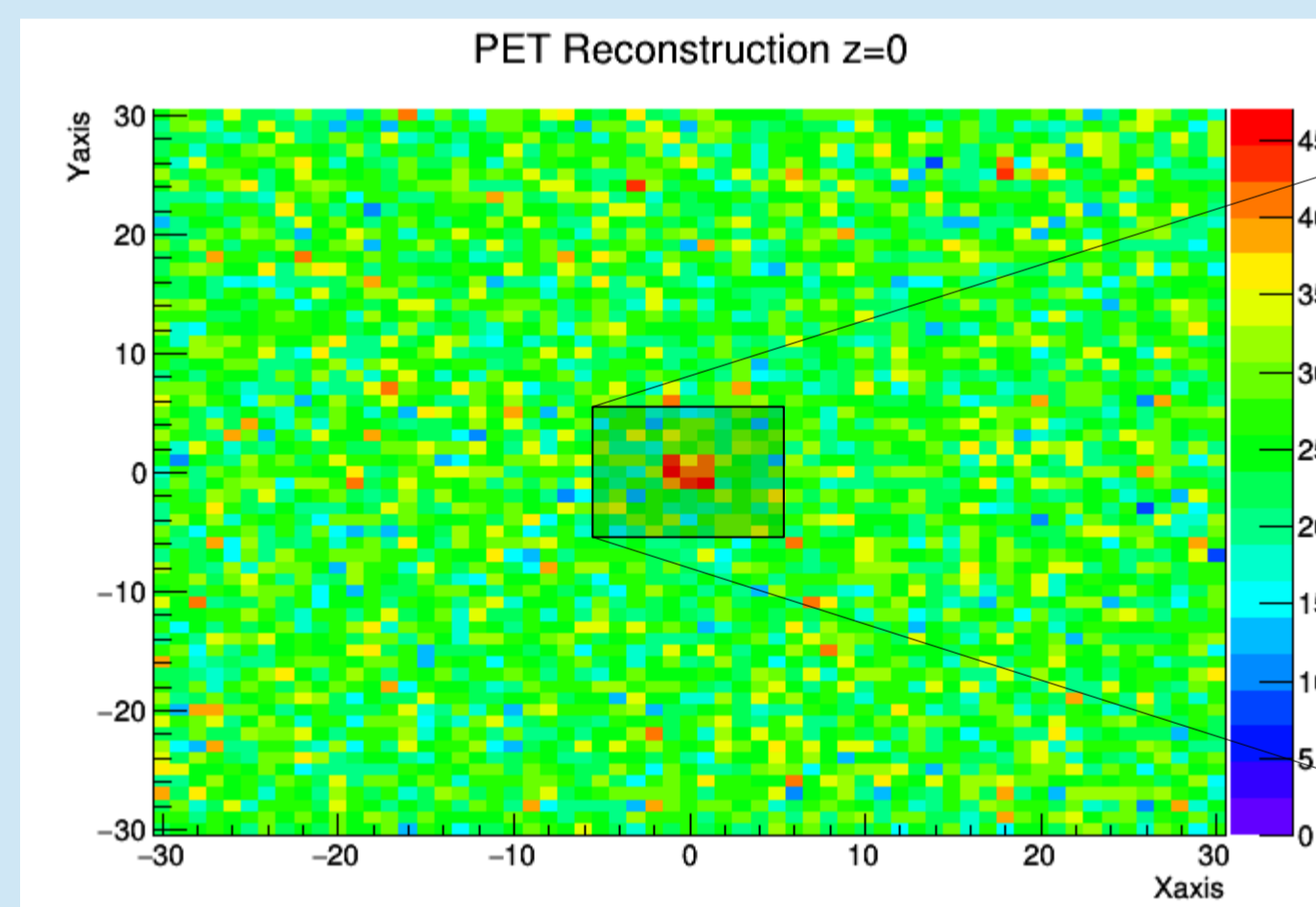
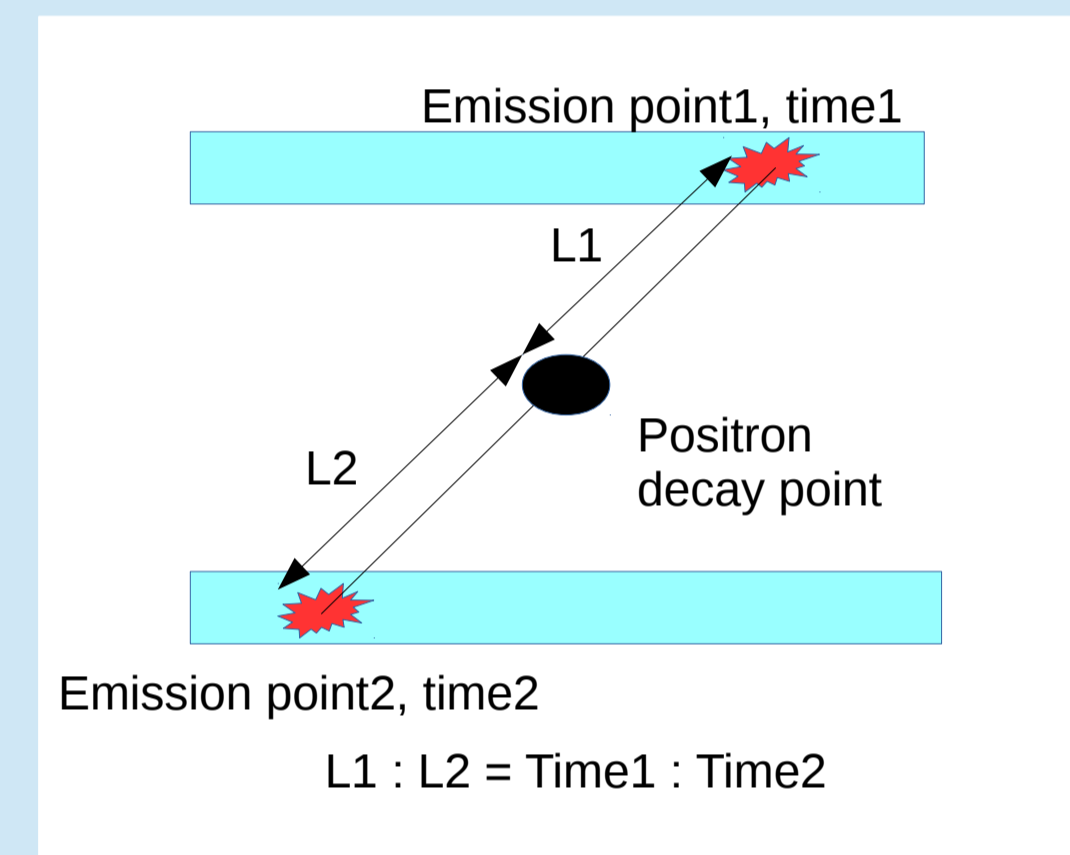
- Positron energy : ¹⁸F decay energy
- Detector : 1 mm thickness La-GPS × 24 layers × 6 detectors
- Cancer area : 3 mm × 3 mm × 3 mm cube, center of human
- Energy threshold : 430 – 590 keV

Reconstructing method

- ① Measuring 430 - 590 keV in 2 detectors
- ② Analyzing first emission points (scattering event : adopting nearest point to the body)
- ③ Calculating positron decay point by the method in left figure

$$pos_{decay} = \frac{time_1 pos_2 + time_2 pos_1}{time_1 + time_2}$$

- ④ Filling decay point in histogram (bin-size : 1 mm)

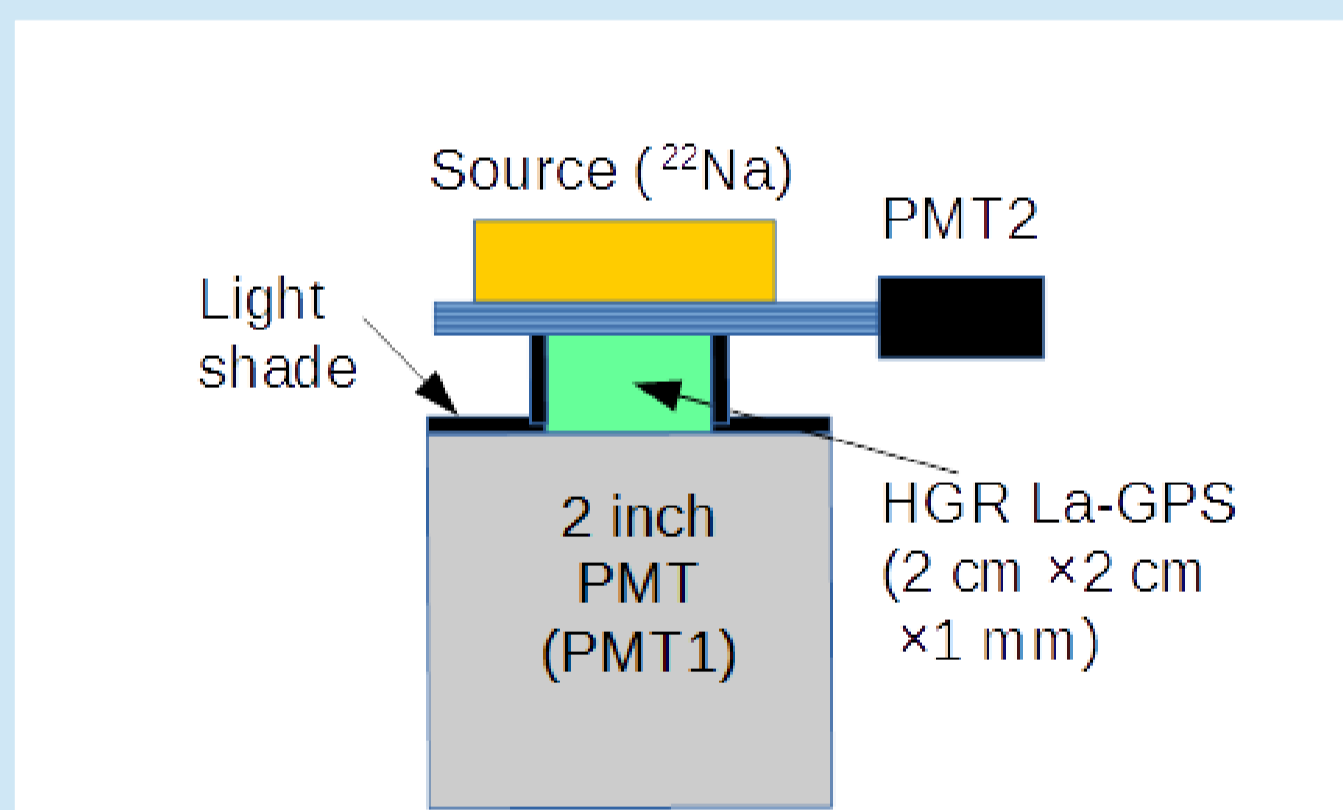


Result

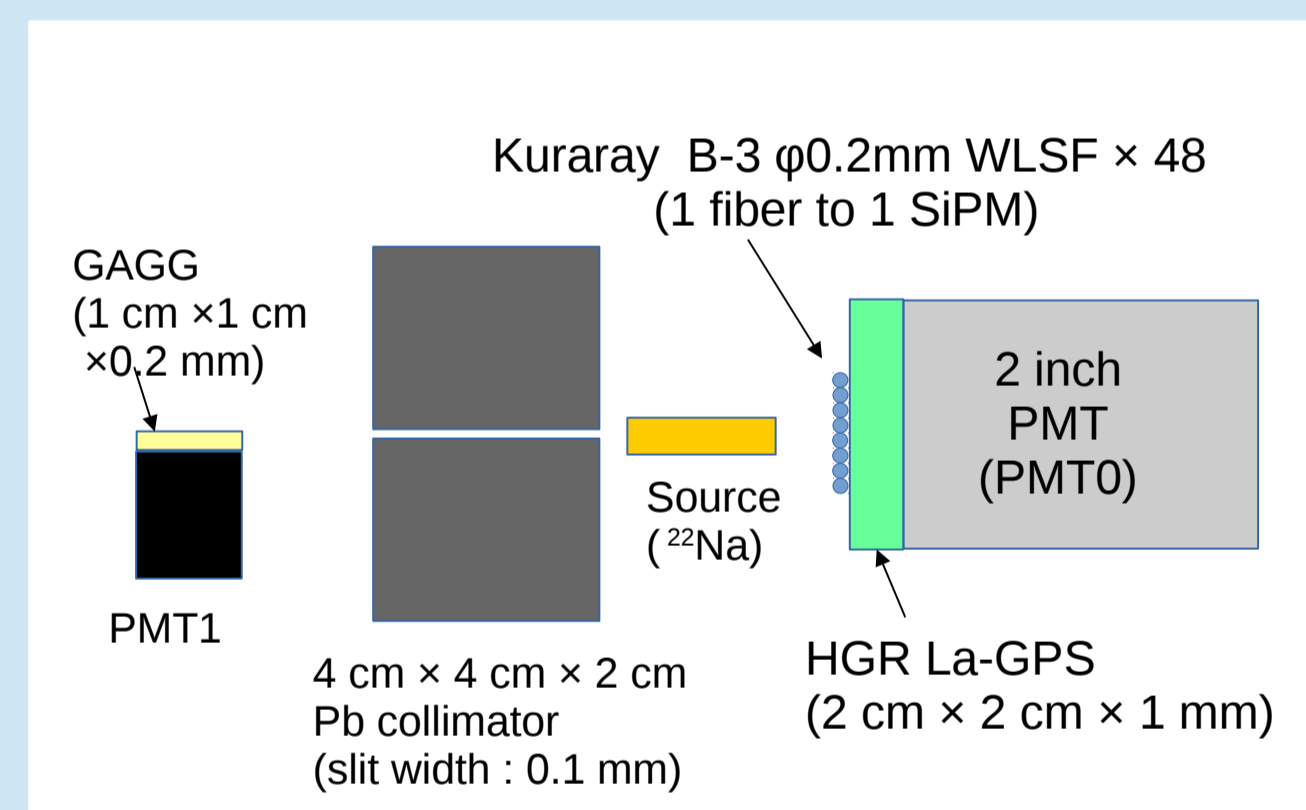
Background level : 25.4 ($\sigma=5.04$)
Cancer level : 17.1

Counts in cancer area are more than 2σ in background.

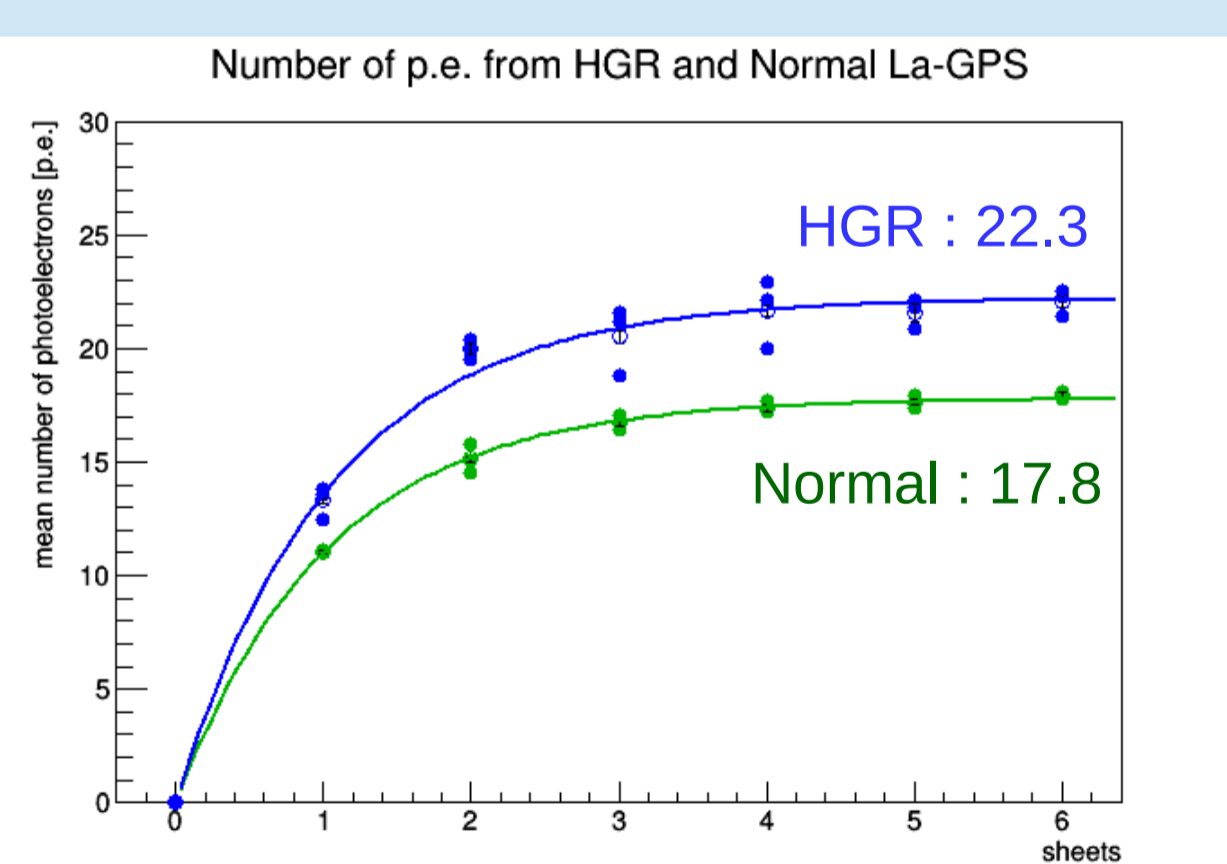
Experiment



Exp. 1. Measurement of energy resolution



Exp. 2. Measurement of position resolution

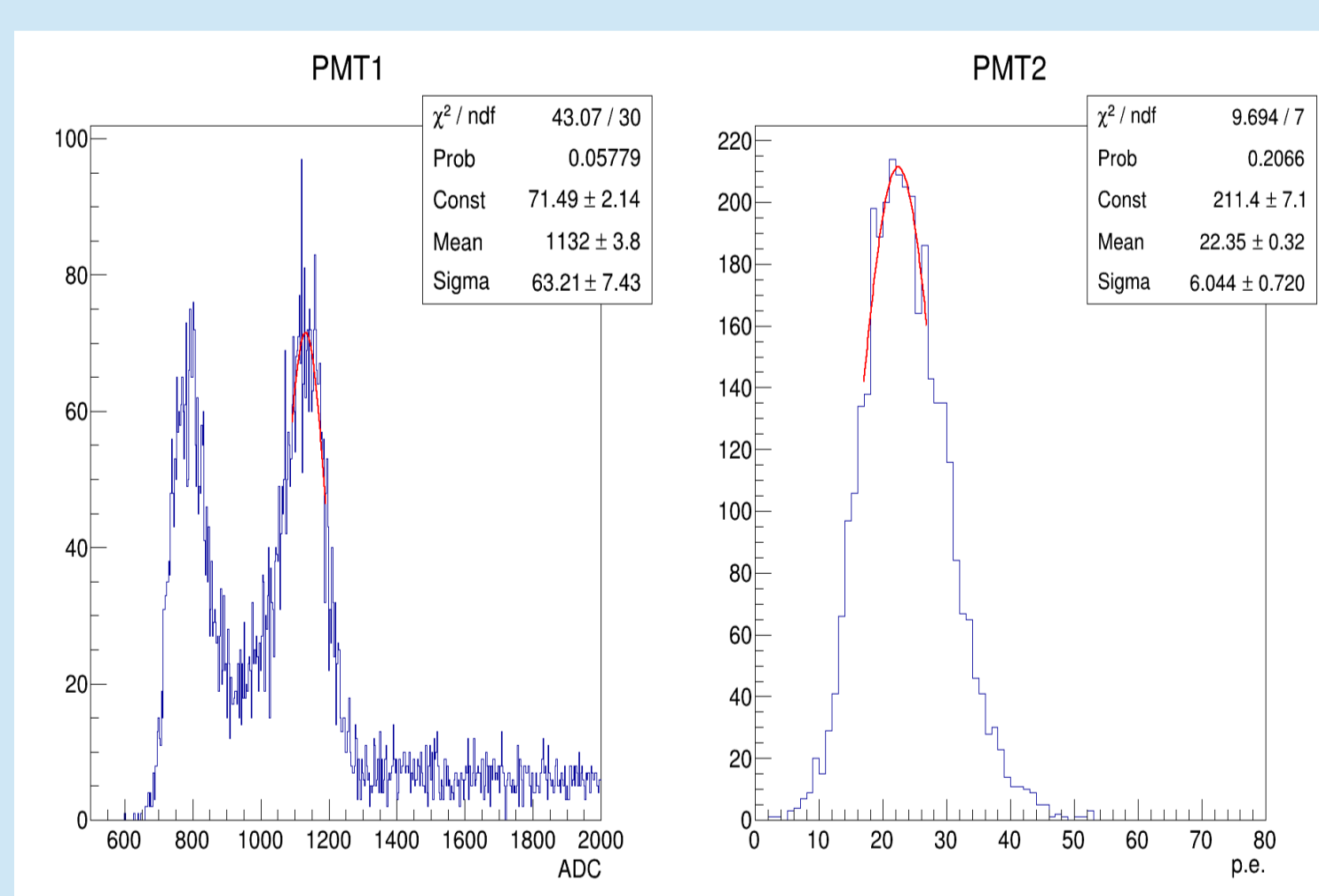


Exp. 1. result

p.e. in 511-keV : 22.3 ± 5.96 (σ)
(HGR, single-face, single-end)

↓

89.2 ± 11.9 (σ)
(double-faces, double-ends)
Energy resolution : 31.4% (FWHM)
cf. p.e. in 511-keV with normal crystal : 17.8



Exp. 2.

Analysis method

Centroid method with all SiPMs' output

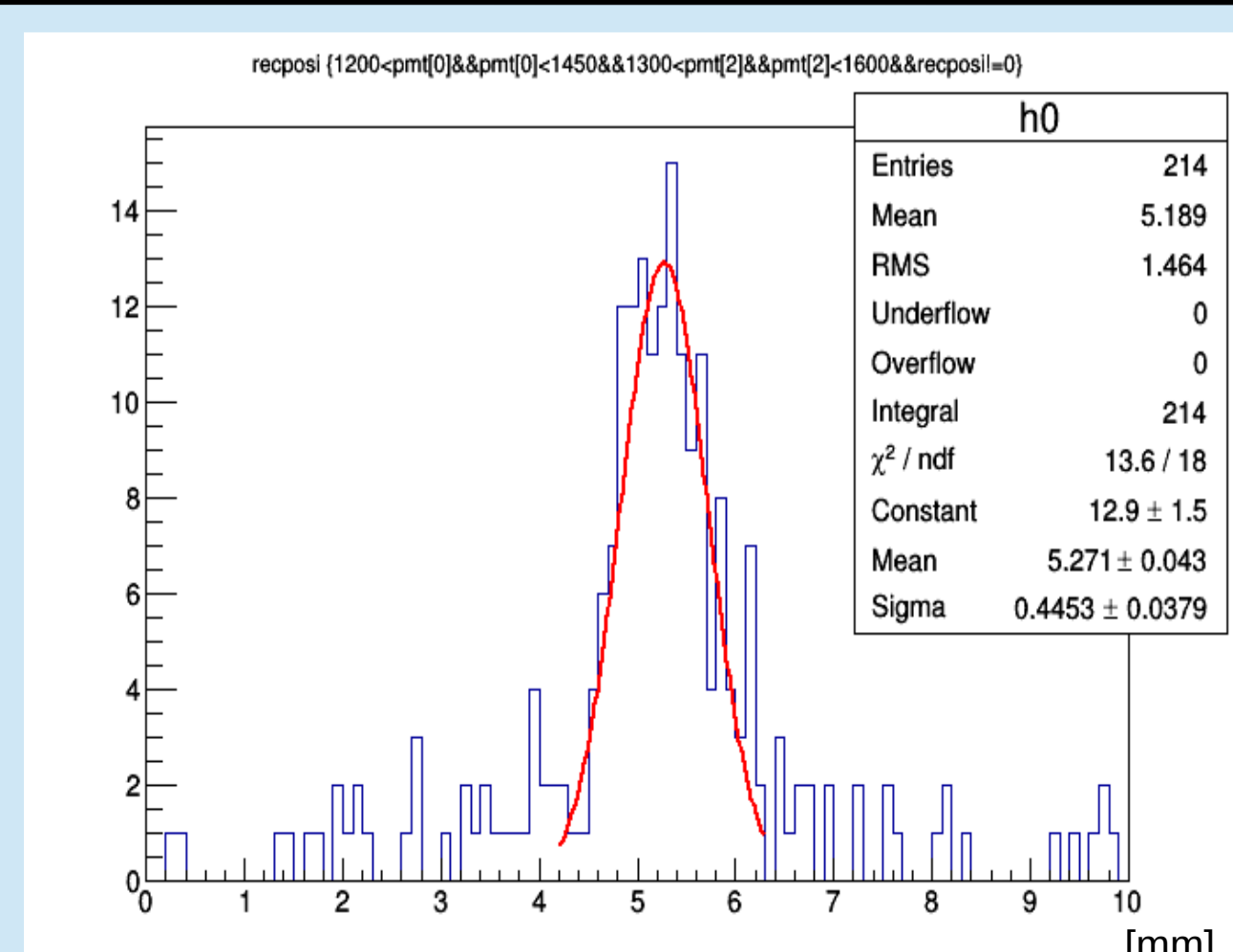
Reconstructing formula :

$$pos_{rec} = \frac{\sum_i n_{p.e.,i} \times \left(\frac{10.0}{48} \times (i+0.5) \right)}{\sum_i n_{p.e.,i}} [mm]$$

(i : SiPM's number)

result

Position resolution : 1.04 mm (FWHM)



Discussion and conclusion

• Our prototype detector, including plate-like HGR La-GPS and WLSF sheets, has 31.4% energy resolution and 1.04 mm position resolution. In GEANT4 simulation, it is confirmed that these parameters are sufficient for identifying 3 mm cancer.

• Setup of exp. 2. has a problem about the width of 511-keV gamma rays from ²²Na source. Positrons from ²²Na is spread out in acrylic part of source. This is an critical issue.

Reference

- [1] Berger M J; Hubbell J H; Seltzer S M; Chang J; Coursey J S; Sukumar R; Zucker D S; Olsen K: NIST XCOM: Photon Cross Section Database
<http://physics.nist.gov/PhysRefData/Xcom/html/xcom1.html>
(retrieved on the 8th of May 2017)

Acknowledgement

We would like to thank C&A corp. for providing La-GPS scintillators.